

Statistical Methods for Online Monitoring in Intensive Care

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joint work with

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Wiebke Sieben



SFB 475: Reduction of Complexity
in Multivariate Data Structures

tu technische universität
dortmund

Collaborative Research Centre SFB 475

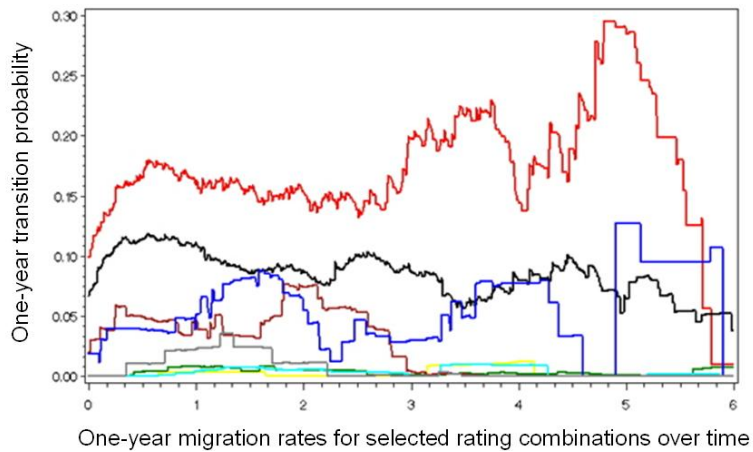
- Reduction of Complexity in Multivariate Data Structures -

Complex scientific problems in economics, engineering & life sciences

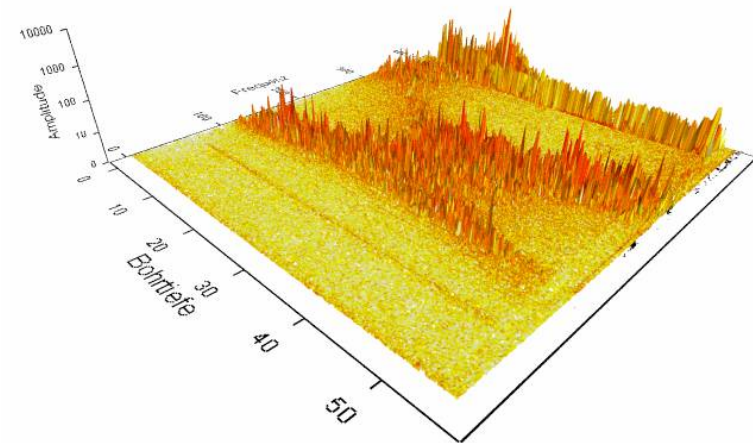
- Analysis of capital and labor markets
- Quality control in complex production processes
- Online monitoring in intensive care
- Causality of chronic diseases (cancer)

Complex Data Structures

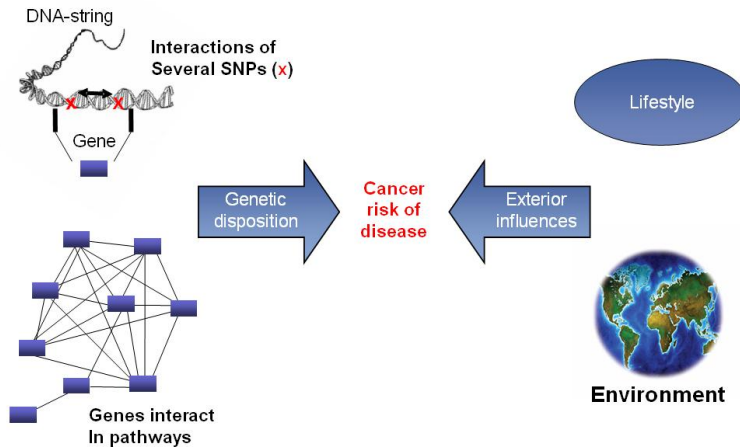
High dynamics



High dimensions

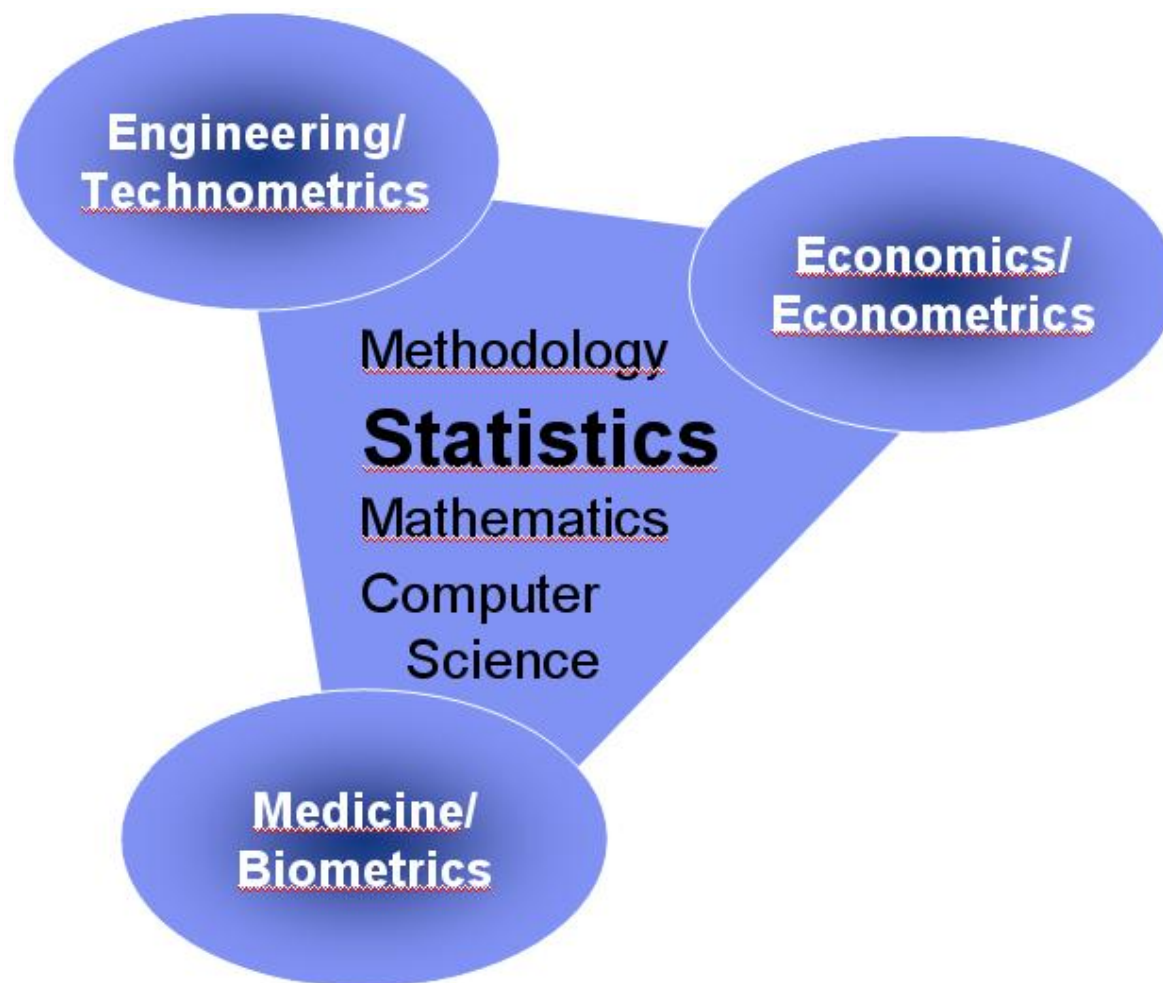


Complex dependence structures



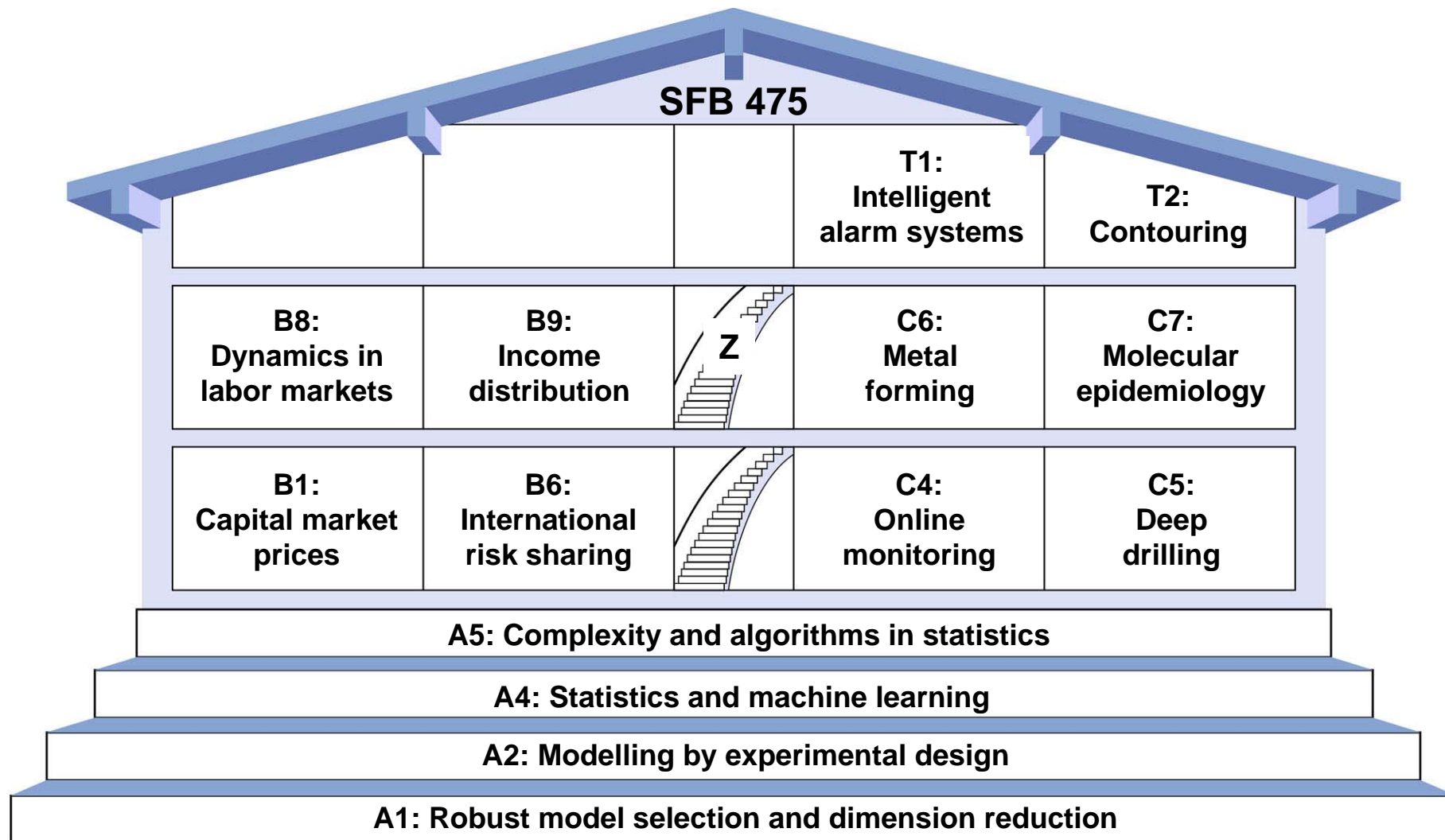
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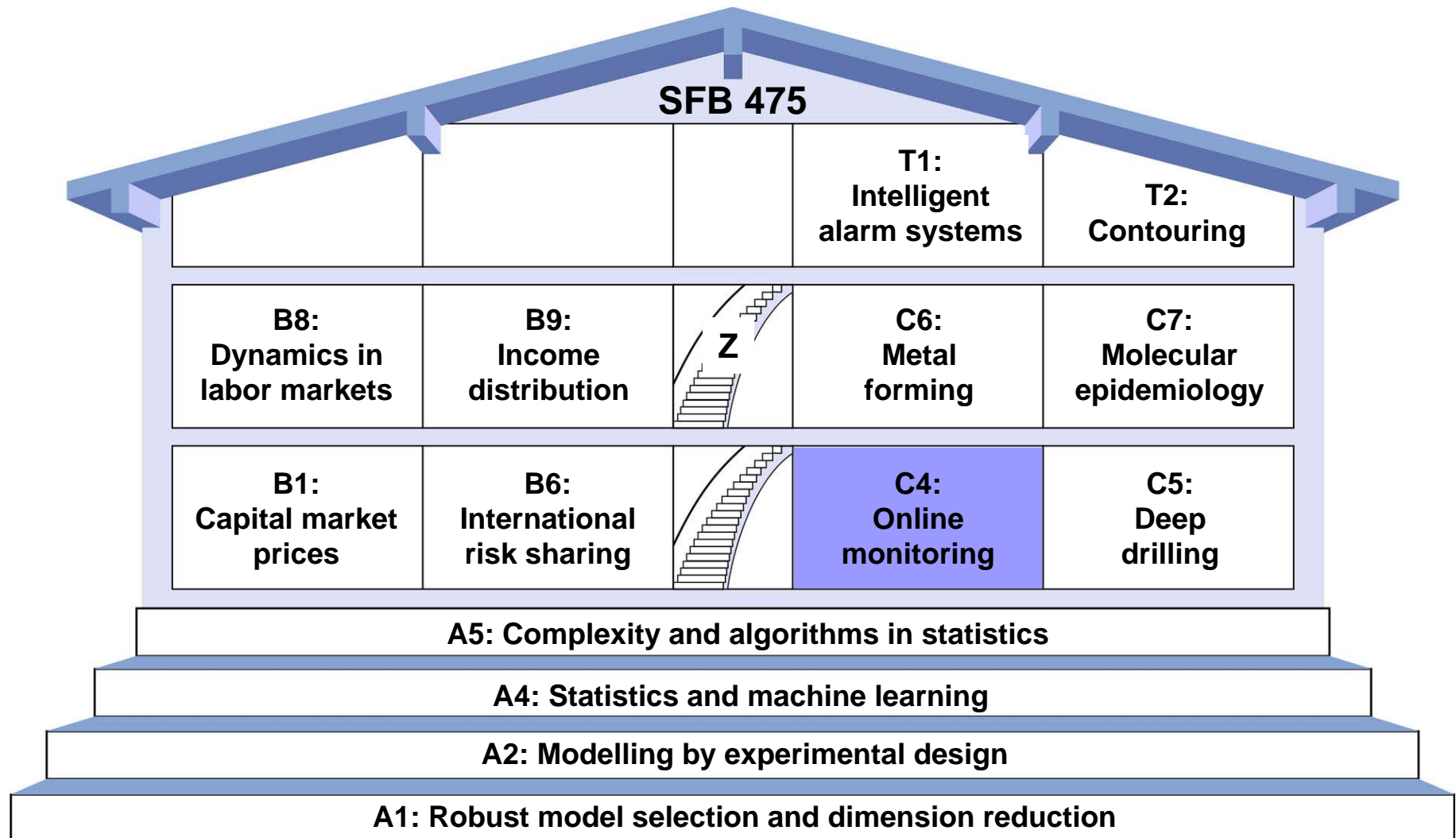
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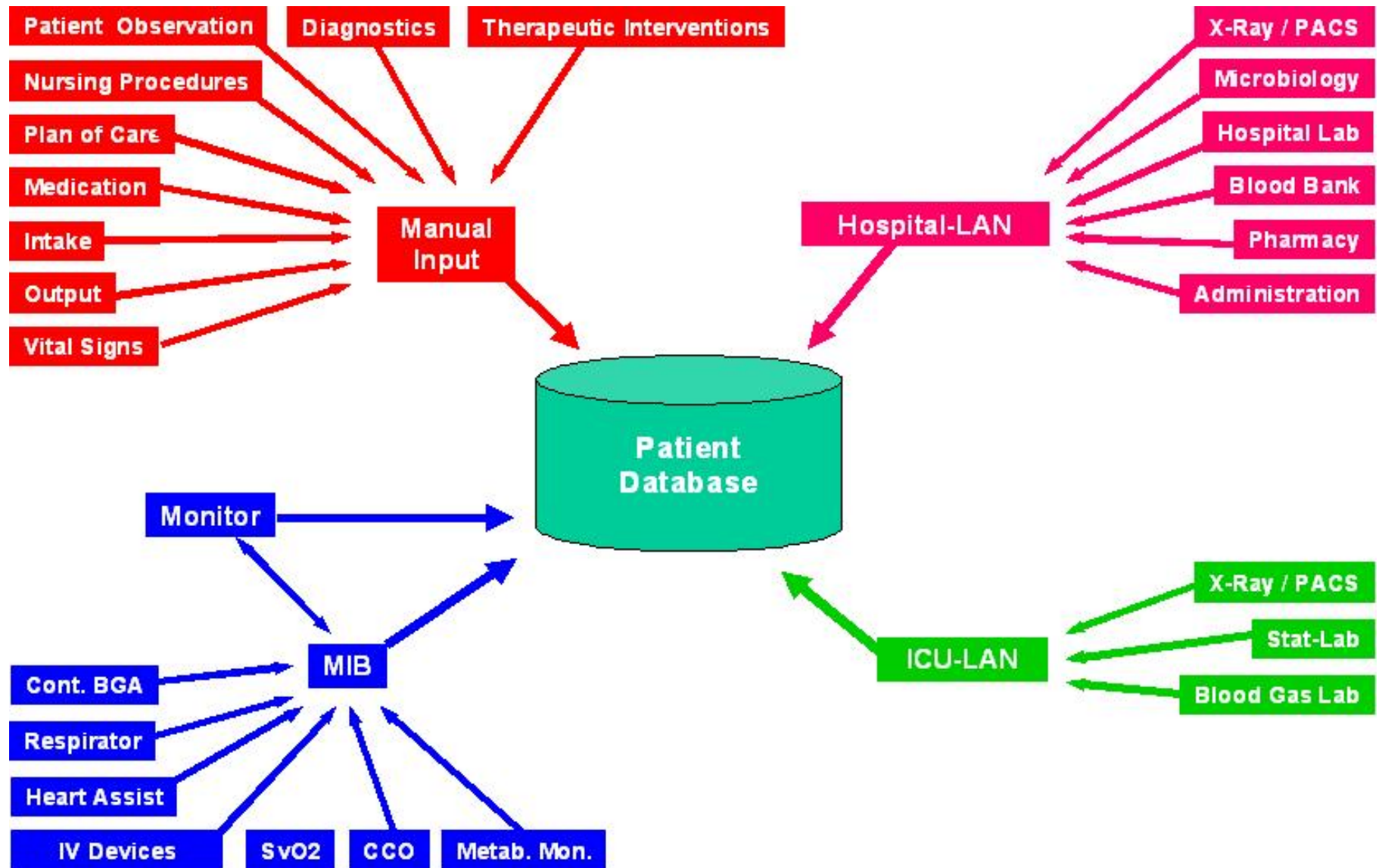
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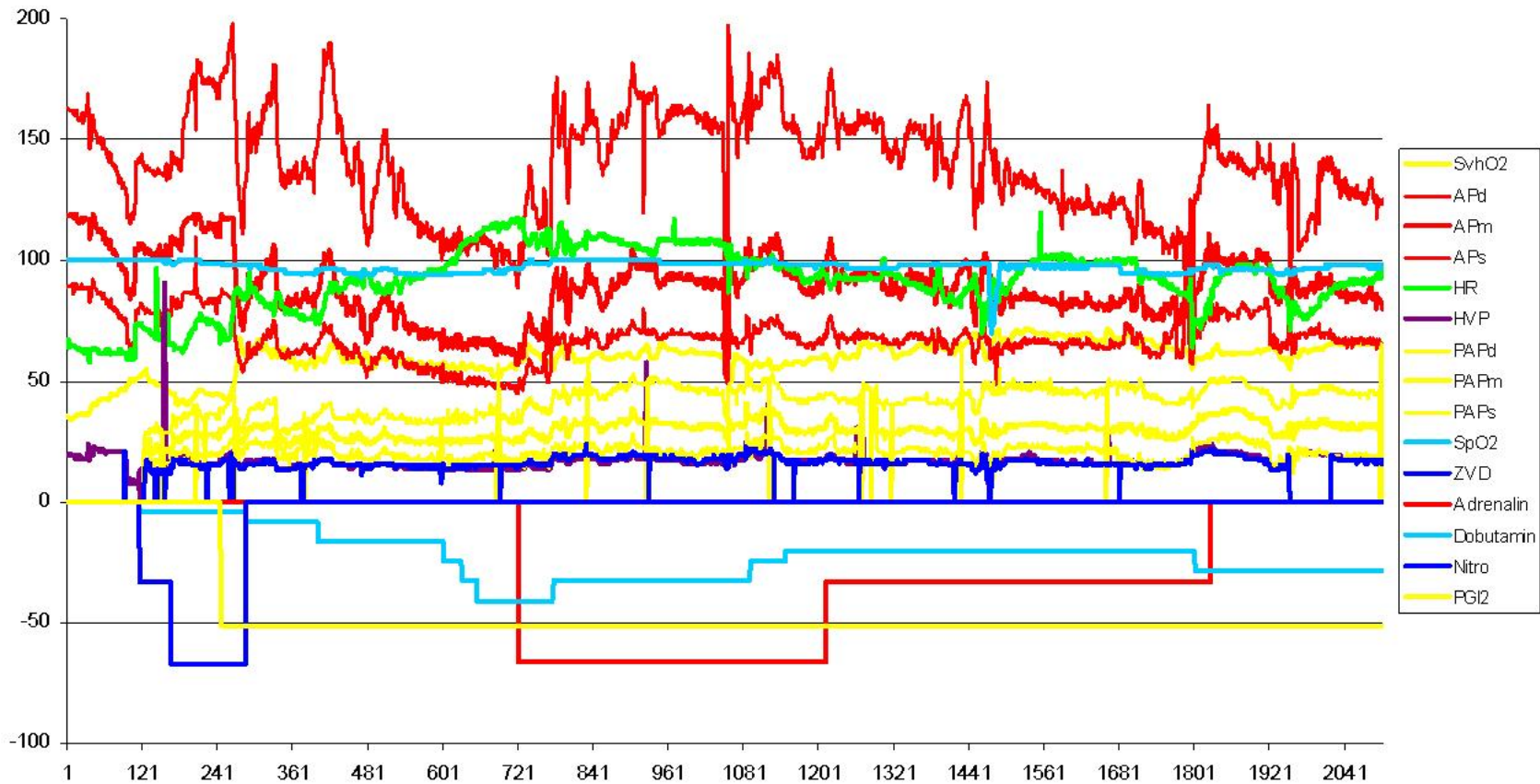
Intensive Care



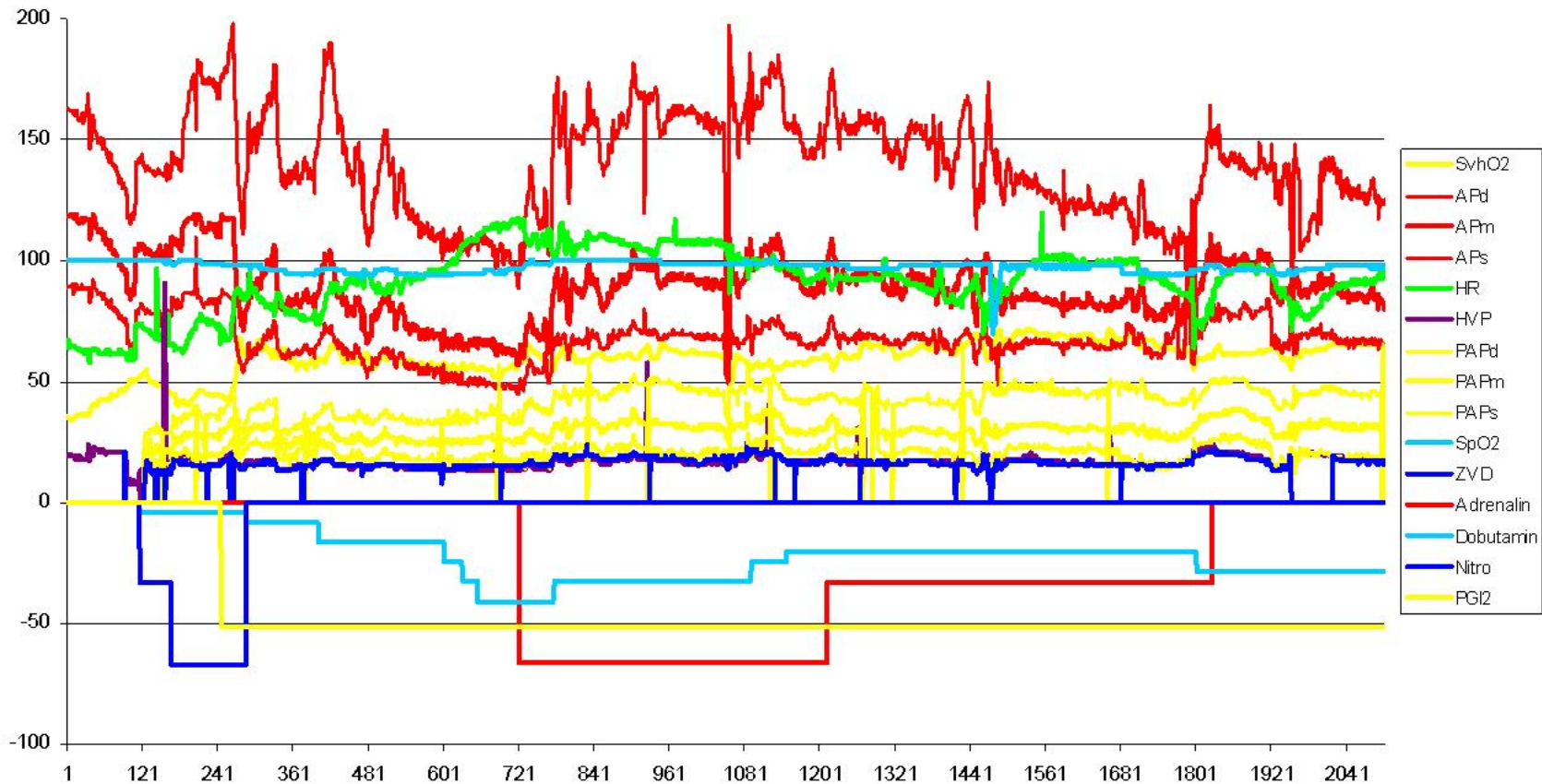
Data Acquisition



Motivation: Multivariate Time Series



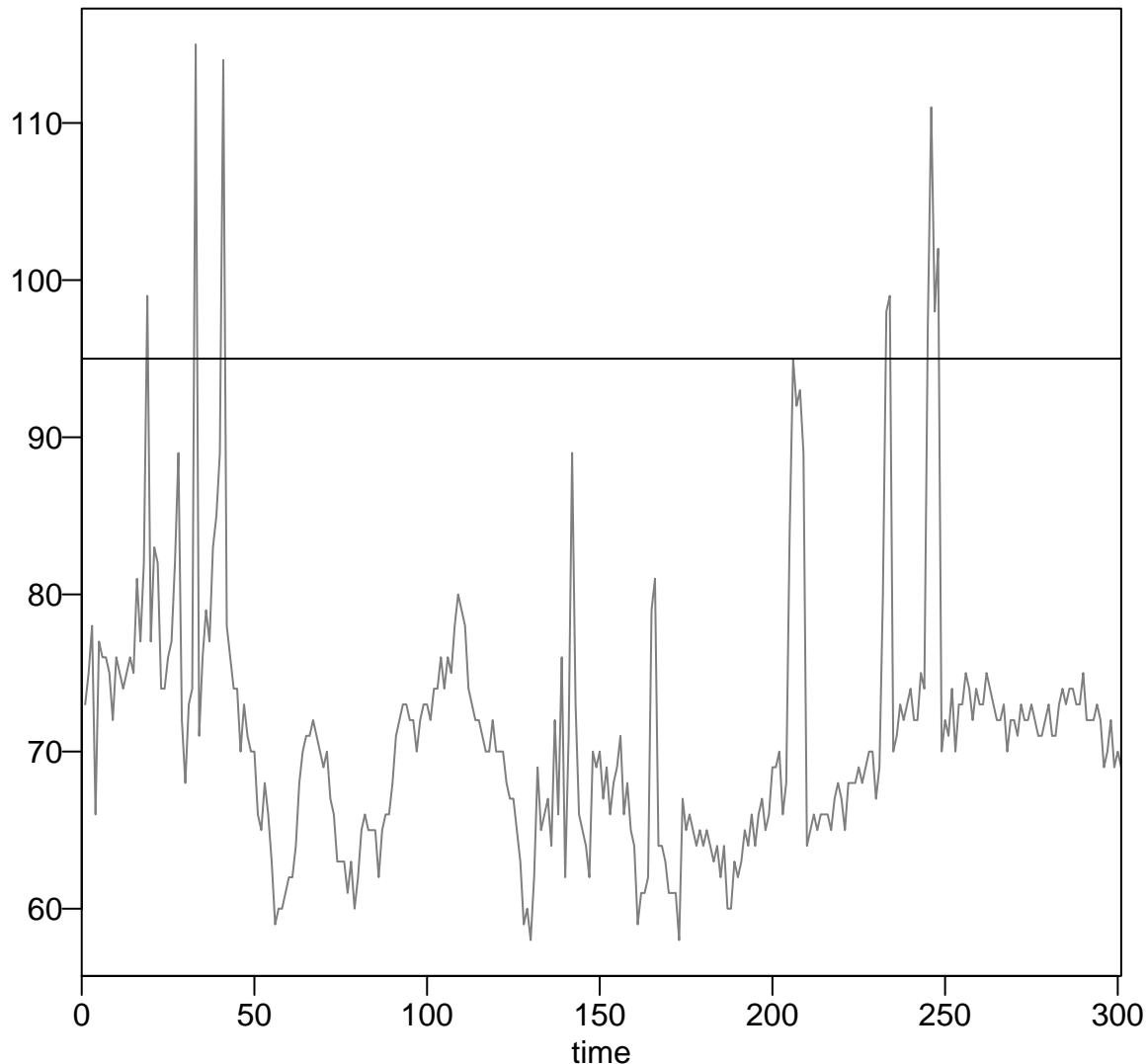
Motivation: Multivariate Time Series



Objective: Online extraction of clinically relevant information from multivariate time series of the haemodynamic system

Motivation: Univariate Signal Extraction

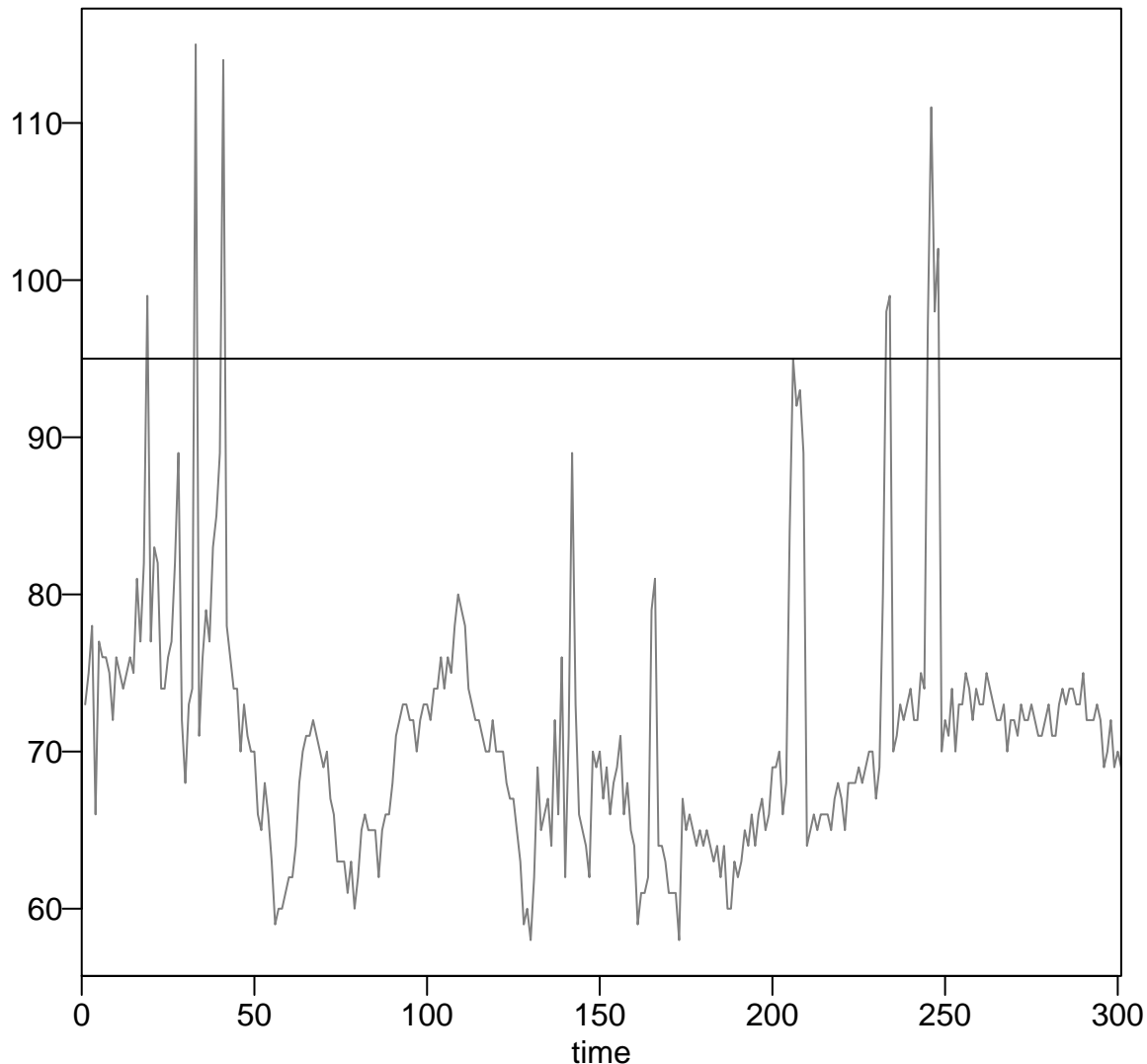
Mean Arterial Blood Pressure



- Sudden changes and trends, no steady state
- Many artefacts
⇒ False alarms

Motivation: Univariate Signal Extraction

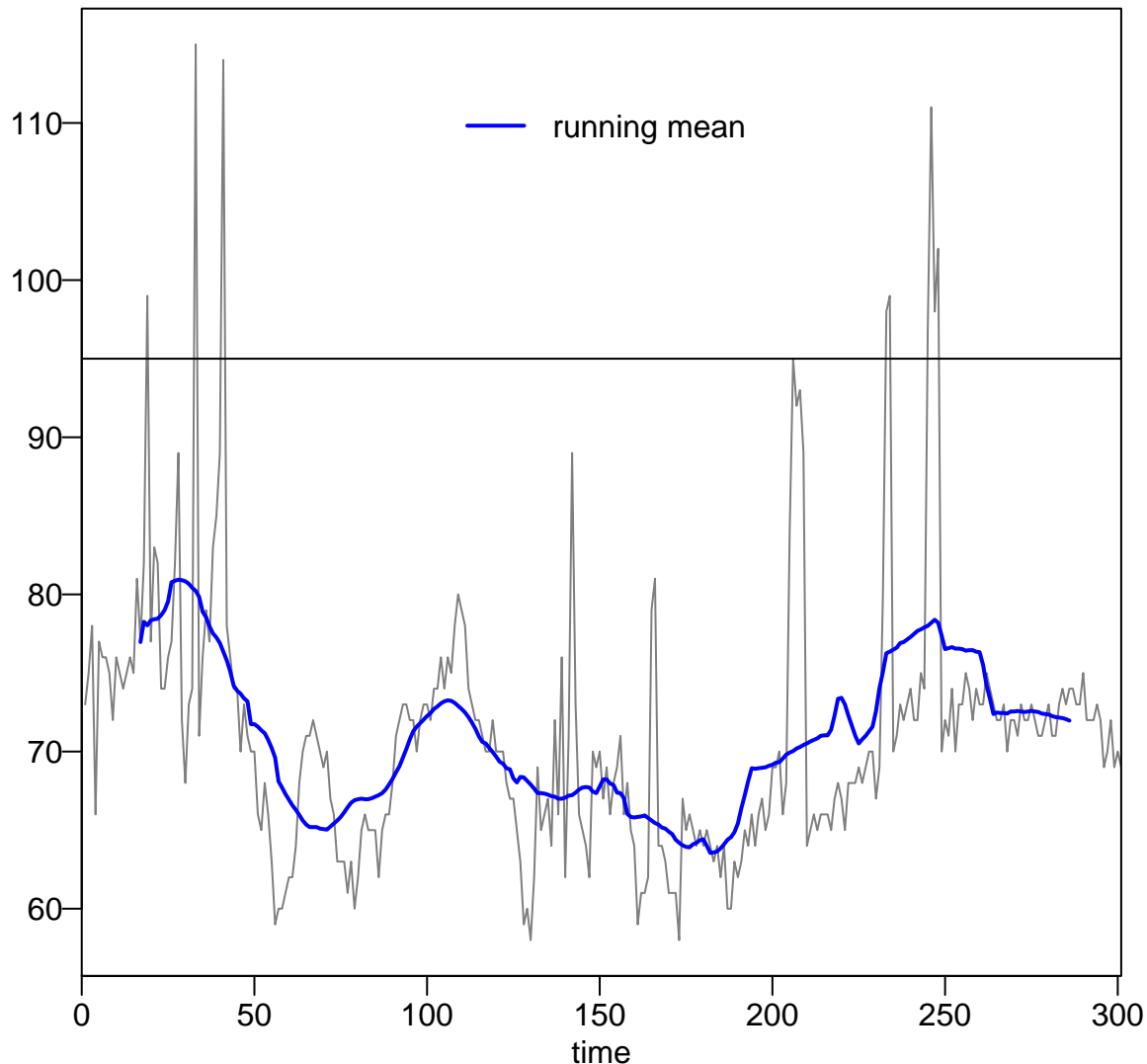
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- New alarm system based on 'correct' signal extraction

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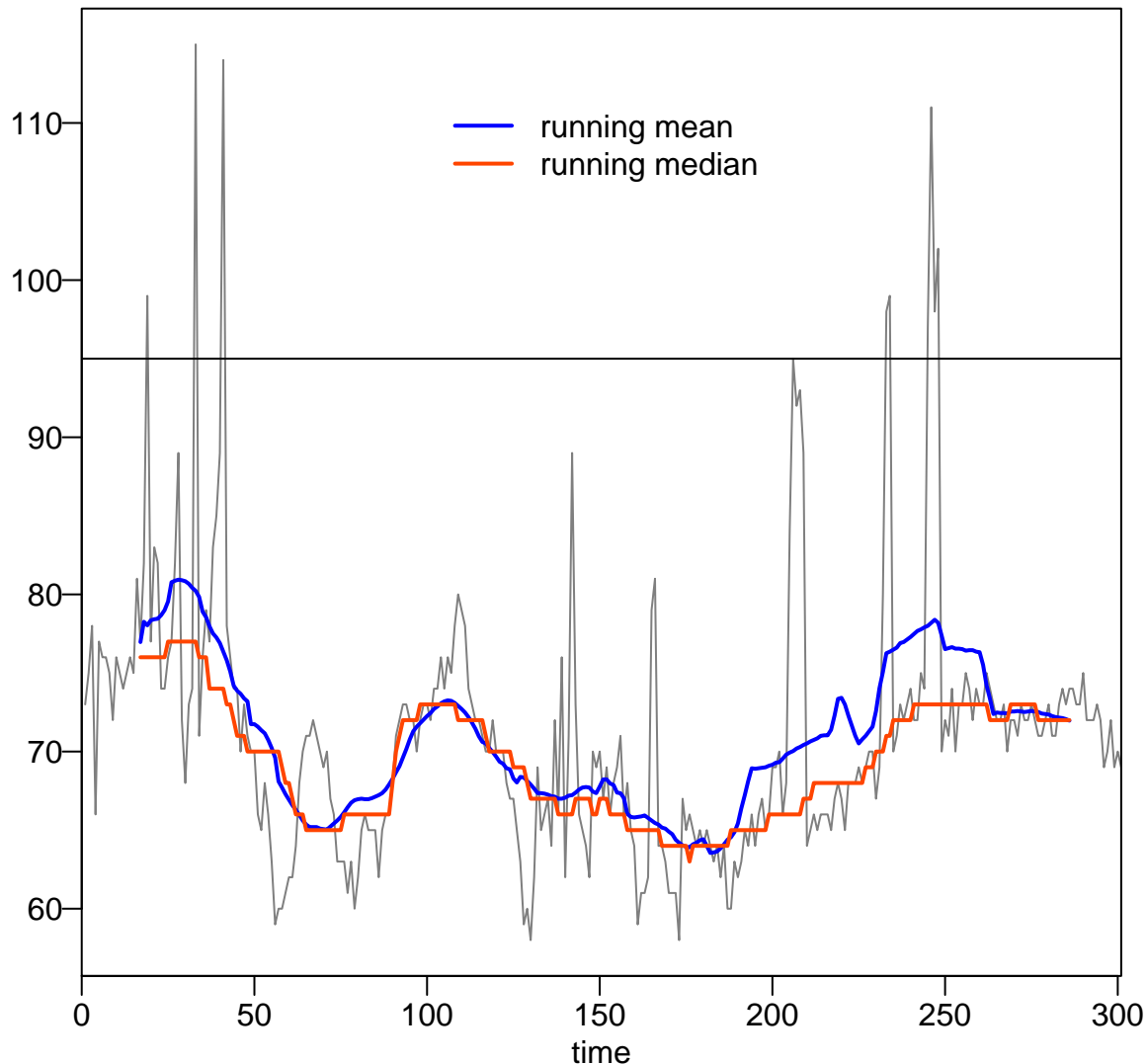
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- Location based filters:
 - Running mean not robust

Motivation: Univariate Signal Extraction

Mean Arterial Blood Pressure



- Sudden changes and trends, no steady state
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⇒ False alarms
- New alarm system based on 'correct' signal extraction
- Location based filters:
 - Running mean not robust
 - Running median not smooth

Challenges

- Trends and level shifts in the signal
- Robustness against outliers
- Unknown dependence structures
- Short time delay
- Short computation time

Overview

I. Univariate signal extraction

- Methods
- Comparisons
- Applications

Overview

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- Applications

II. Multivariate signal extraction

- Methods
- Applications

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II. Multivariate signal extraction

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III. Alarm classification

I. Univariate Signal Extraction

Signal Extraction from Univariate Time Series

(Davies, Fried, Gather, 2004)

Model

$$x_t = \mu_t + \epsilon_t + \nu_t, \quad t \in \mathbb{N}$$

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Signal

smooth with a
few sudden shifts

Observational noise

symmetric
mean zero

Spiky noise

measurement
artefacts, ...

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artefacts, ...

Idea

Take moving windows $\{x_{t-m}, \dots, x_t, \dots, x_{t+m}\}$ to approximate μ_t

Model: Signal Extraction from Univariate Time Series

Local linear model within a time window of length $n = 2m + 1$:

$$x_{t+i} = \mu_t + \beta_t i + \varepsilon_{t,i}, \quad i = -m, \dots, m$$

- **Estimation of the current level**

either by $\hat{\mu}_t$ in centre or by $\hat{\mu}_{t+m}^{online} = \hat{\mu}_t + \hat{\beta}_t m$

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- ★ Bias and variability \Rightarrow Smoothness
- ★ Robustness against outliers \Rightarrow Stability
- ★ Computation time \Rightarrow Speed

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Estimation of level μ_t and slope β_t by robust linear regression

Robust Regression Methods

Repeated Median (RM)

(Siegel, 1982)

$$\hat{\beta}_t^{\text{RM}} = \text{med}_{i=-m}^m \left\{ \text{med}_{j \neq i} \frac{y_i - y_j}{i - j} \right\}$$

$$\hat{\mu}_t^{\text{RM}} = \text{med}_{i=-m}^m \left\{ x_{t+i} - \hat{\beta}_t^{\text{RM}} i \right\}$$

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$$\hat{\mu}_t^{\text{RM}} = \text{med}_{i=-m}^m \left\{ x_{t+i} - \hat{\beta}_t^{\text{RM}} i \right\}$$

Least Median of Squares (LMS)

(Hampel, 1975; Rousseeuw, 1984)

$$(\hat{\mu}_t^{\text{LMS}}, \hat{\beta}_t^{\text{LMS}})' = \arg \min_{\hat{\mu}_t, \hat{\beta}_t} \left\{ \text{med}_{i=-m}^m \{ r_{t+i}^2 \} \right\}$$

Robust Regression Methods

L_1 -Regression

(Edgeworth, 1887)

$$(\hat{\mu}_t^{L_1}, \hat{\beta}_t^{L_1})' = \arg \min_{\hat{\mu}_t, \hat{\beta}_t} \sum_{i=-m}^m |r_{t+i}|$$

Robust Regression Methods

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Least Trimmed Squares

(Rousseeuw, 1983)

$$(\hat{\mu}_t^{LTS}, \hat{\beta}_t^{LTS})' = \arg \min_{\hat{\mu}_t, \hat{\beta}_t} \sum_{k=1}^{\lfloor n/2 \rfloor + 1} (r_t^2)_{k:n}$$

Robust Regression Methods

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Deepest Regression

(Rousseeuw and Hubert, 1999)

$$(\hat{\mu}_t^{DR}, \hat{\beta}_t^{DR}) = \arg \max_{\hat{\mu}_t, \hat{\beta}_t} \left\{ rdepth \left((\hat{\mu}_t, \hat{\beta}_t), \mathbf{x}_t \right) \right\}$$

Comparisons: Robustness

Smallest number k^* of contaminated observations
which can cause a spike of any size in the extracted signal

$$k^* = \min \{k : \sup\{\|T(\mathbf{z}) - T(\mathbf{x})\|, \mathbf{z} \in U_k(\mathbf{x})\} = \infty\}$$

with $U_k(\mathbf{x}) = \{\mathbf{z} = (z_1, \dots, z_n) : \#\{i : z_i \neq x_{t+i}\} = k\}$

Comparisons: Robustness

Smallest number k^* of contaminated observations which can cause a spike of any size in the extracted signal

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k^*	L₂	L₁	LMS	LTS	RM	DR
$n = 21$	1	7	10	10	10	≥ 6
$n = 31$	1	10	15	15	15	≥ 10

Comparisons: Efficiency

(Gather, Schettlinger, Fried, 2006)

Finite sample efficiencies for the **online estimates** $\hat{\mu}_t^{online}$ relative to Least Squares:

		LMS	LTS	RM	DR
standard normal errors	$n = 21$.23	.22	.71	.62
	$n = 31$.21	.20	.70	.61
rescaled t_3 errors	$n = 21$.58	.56	1.44	1.37
	$n = 31$.58	.57	1.50	1.42
shifted lognormal errors	$n = 21$.44	.43	1.00	.93
	$n = 31$.35	.33	.85	.78

→ Similar results for **LMS** & **LTS** and **RM** & **DR**

→ **RM** best

Comparisons: Computation Times

Simulated mean computation time of an update in milliseconds

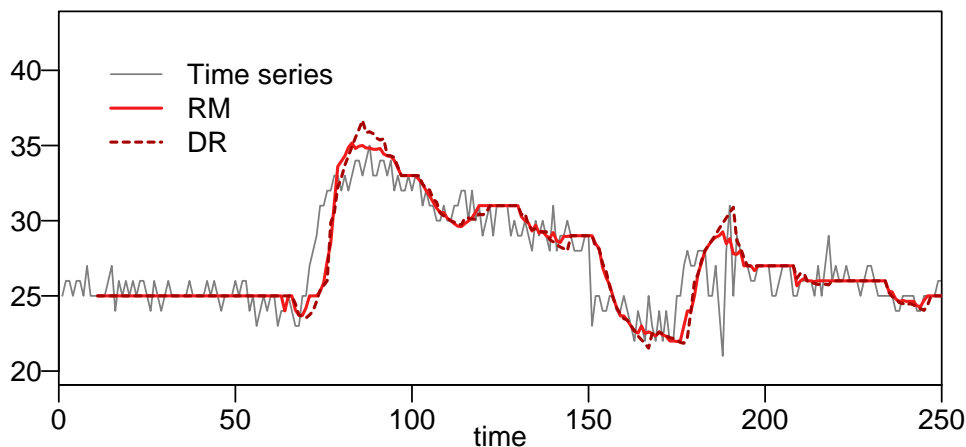
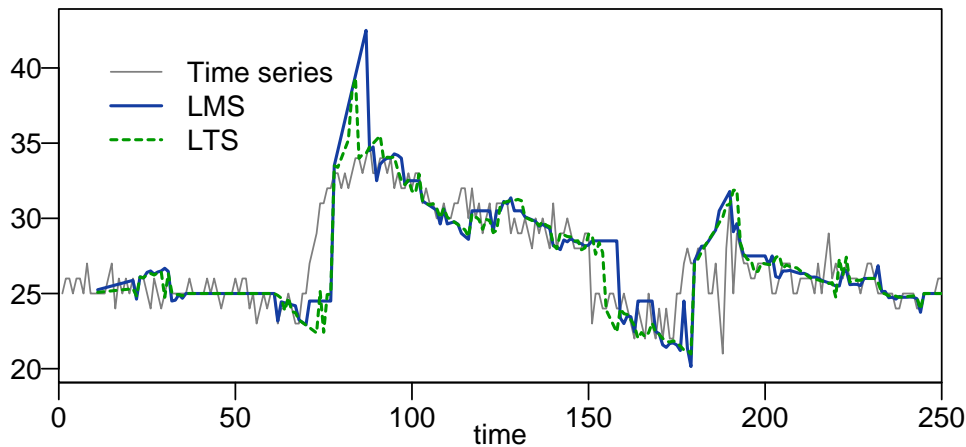
	LMS	LTS	RM	DR
$n = 21$	0.161	0.161	0.035	0.747
$n = 31$	0.323	0.324	0.049	0.956

Asymptotic computation time for an update

	LMS	LTS	RM	DR
Time	$O(n^2)$	$O(n^2)$	$O(n)$	$O(n \log^2 n)$
Memory space	$O(n^2)$	$O(n^2)$	$O(n^2)$	$O(n)$

Comparisons: Application to Real Data

Mean Pulmonary Artery Blood Pressure



Good performance
of all methods

in *constant* periods

Overestimation of the signal
after the shift for **LMS/LTS**

RM/DR 'blur' shifts

LMS/LTS more affected
by moderate data variation

RM/DR smoother

Summary

Robust regression works well for online signal extraction

- **LMS/LTS** preserve shifts but are unstable and perform poorly for trend changes
- **RM/DR** are stable and good at trend changes but smear shifts
- **RM** fastest, **DR** slowest method

Summary

Robust regression works well for online signal extraction

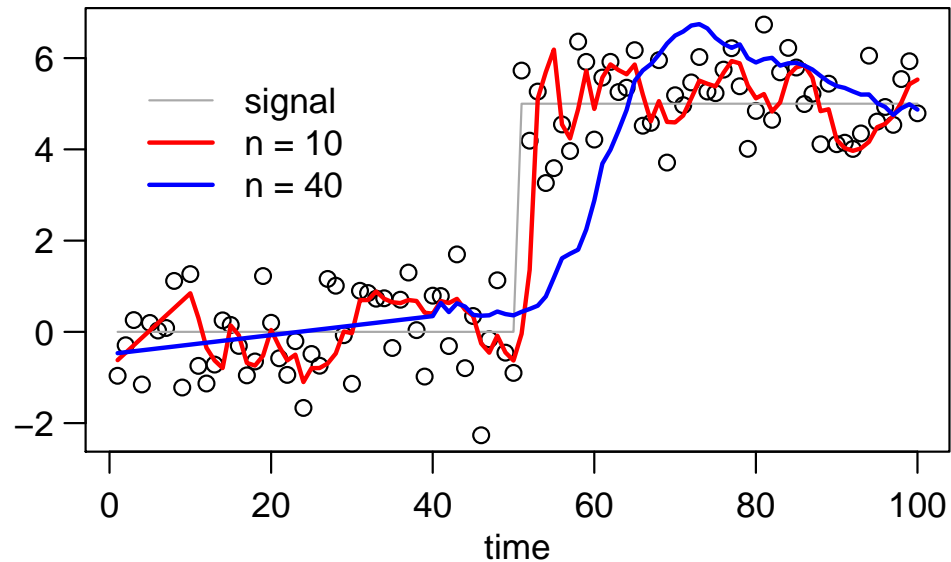
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Overall best performance: RM regression

Improvements and Modifications

- Online outlier replacement and shift detection (Fried, 2004)
- Double window filters: (Bernholt, Fried, Gather, Wegener, 2006)
Trimming based on robust estimate from (smaller) inner window;
Final estimate from outer window
- Hybrid filters: (Fried, Bernholt, Gather, 2006)
Combinations of subfilters applied to window halves
- Weighted repeated median filters (Fried, Einbeck, Gather, 2007)
- Adaptive window widths (Schettlinger, Fried, Gather, 2008)
- ➔ **R** package `robfilter` (Fried, Schettlinger, 2008)

Influence of the Window Width



n small

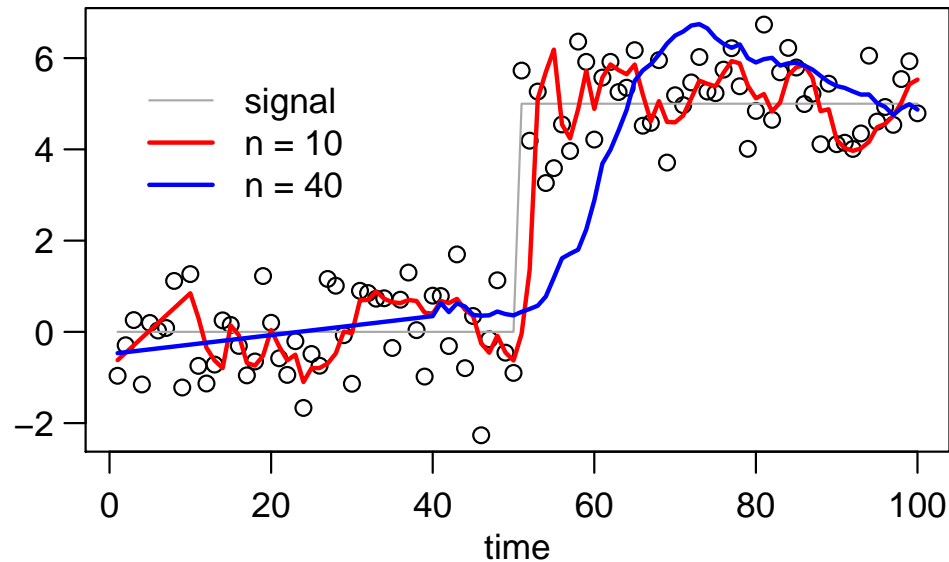
- small bias
- adapts quickly to changes
- short computation time

⇔

n large

- small variance
- smooth
- robust

Influence of the Window Width



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➔ **Data adaptive choice of window width wanted**

Adaptive Choice of Window Width

(Schettlinger, Fried, Gather, 2008)

Idea

Use the 'balance' of the residual signs $\left(\sum_{i=1}^n \text{sign}(r_i) = 0 \right)$

RM approximation in current time window

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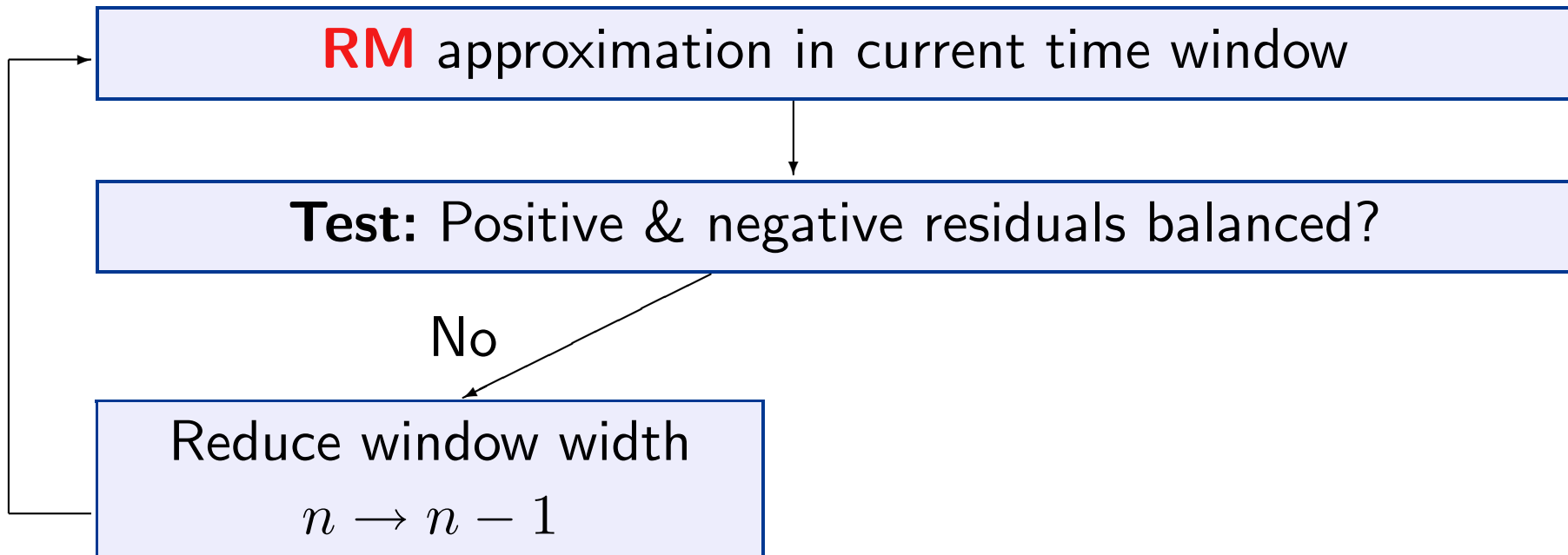
Test: Positive & negative residuals balanced?

Adaptive Choice of Window Width

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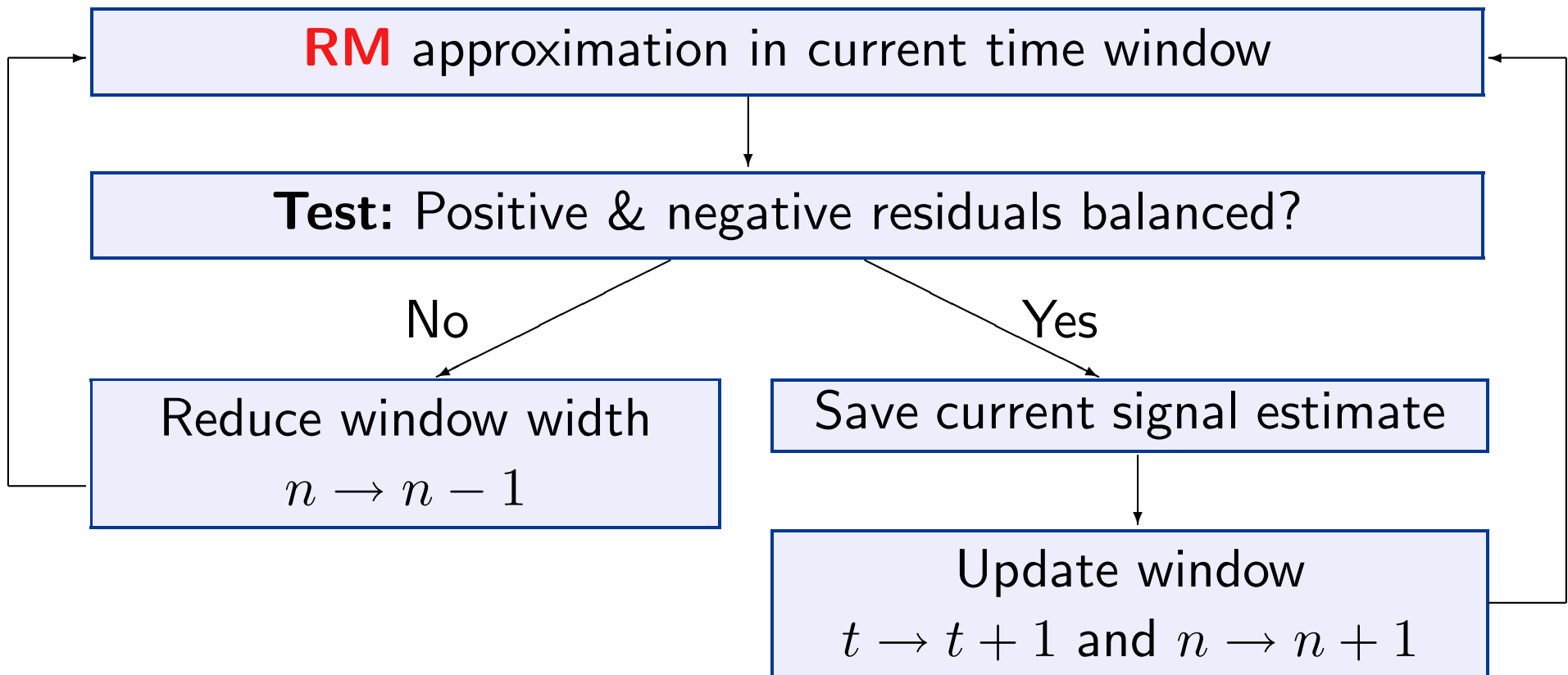


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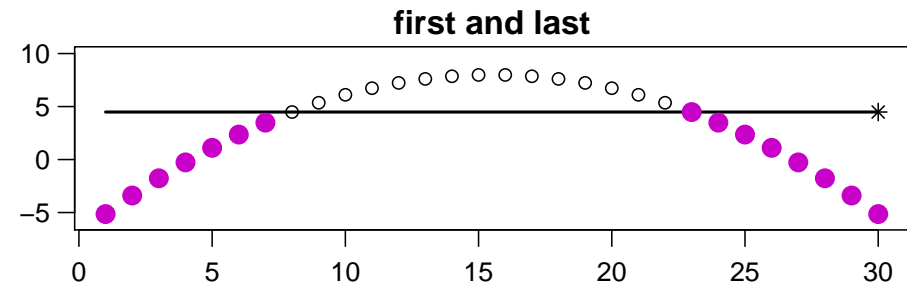
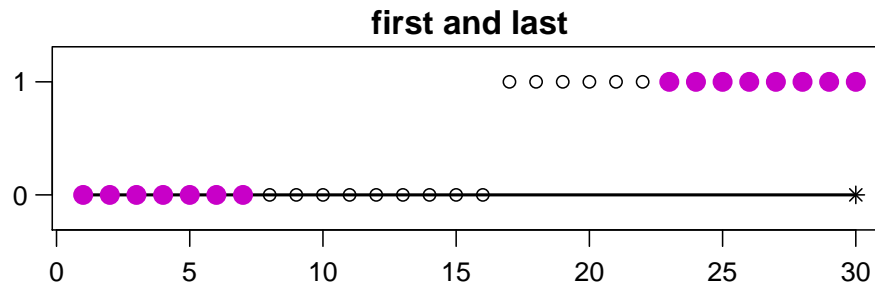
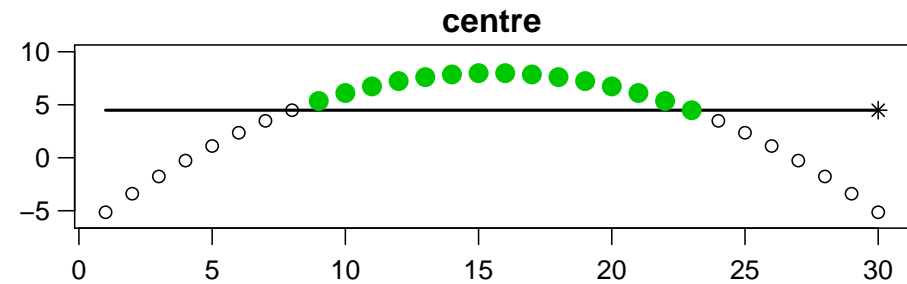
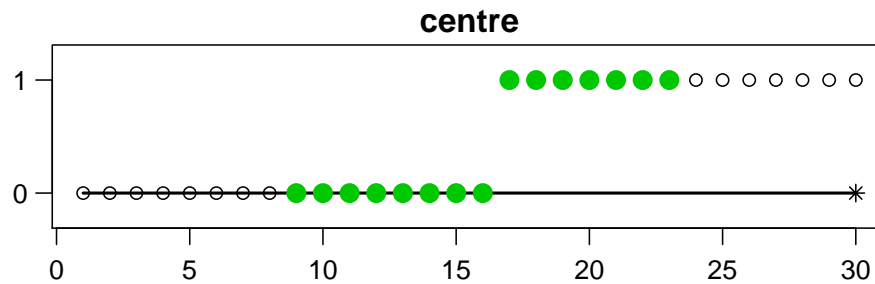
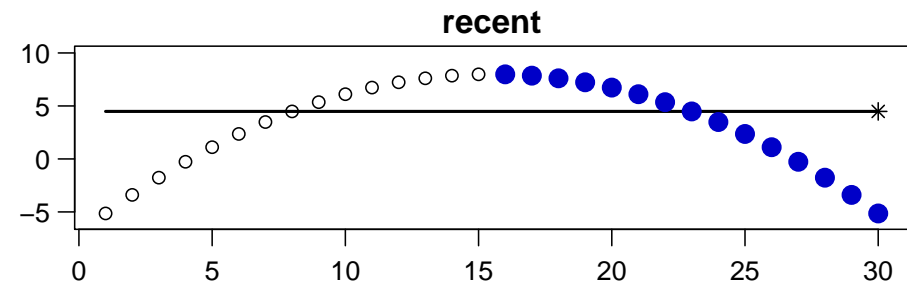
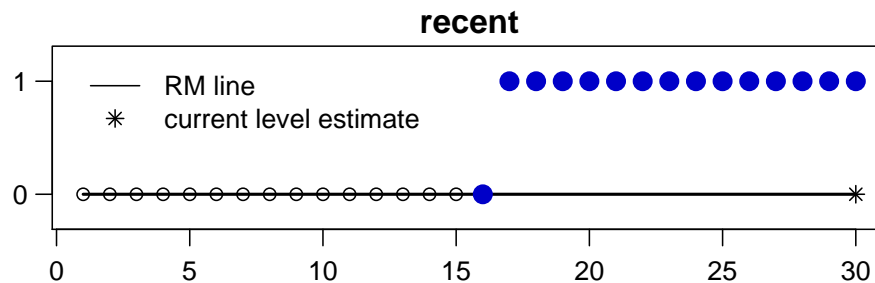
Idea

Use the 'balance' of the residual signs $\left(\sum_{i=1}^n \text{sign}(r_i) = 0 \right)$



Selection of Residuals: Different Sets of Indices I

Example: $n = 30$ with $n_I = \lfloor n/2 \rfloor = 15$ selected time points



➡ Appropriate selection by simulation

Simulation Study

Aims

- Which index set I yields the 'best' results?
- How many values should I contain? $n_I = n/2, n/3, n/4$?
- Should n_I be independent of n ? $n_I = 10, 15, 30$?

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Results

Time delay in tracing a shift / trend change

- for I recent: small $n_I \rightarrow$ small delay
- for I centre / first and last: large $n_I \rightarrow$ small delay

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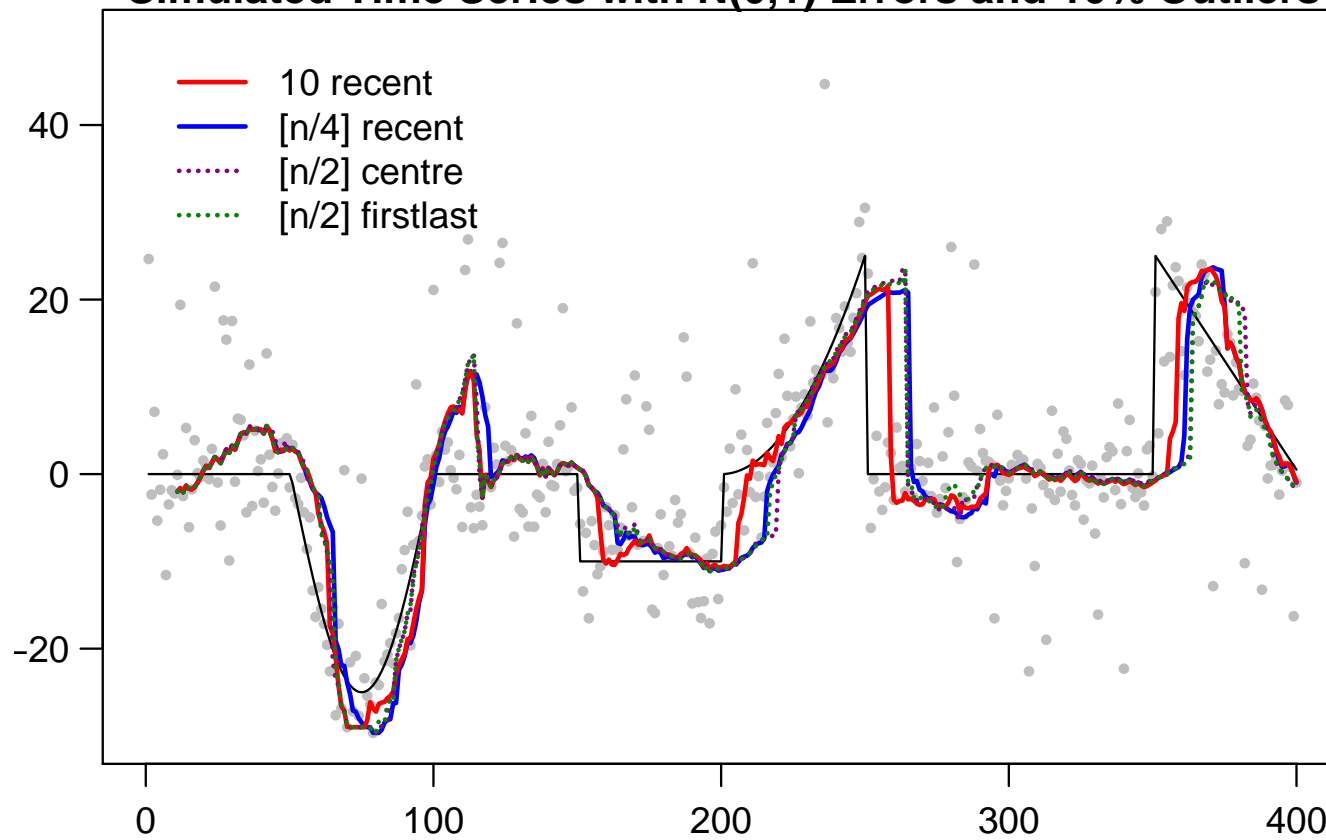
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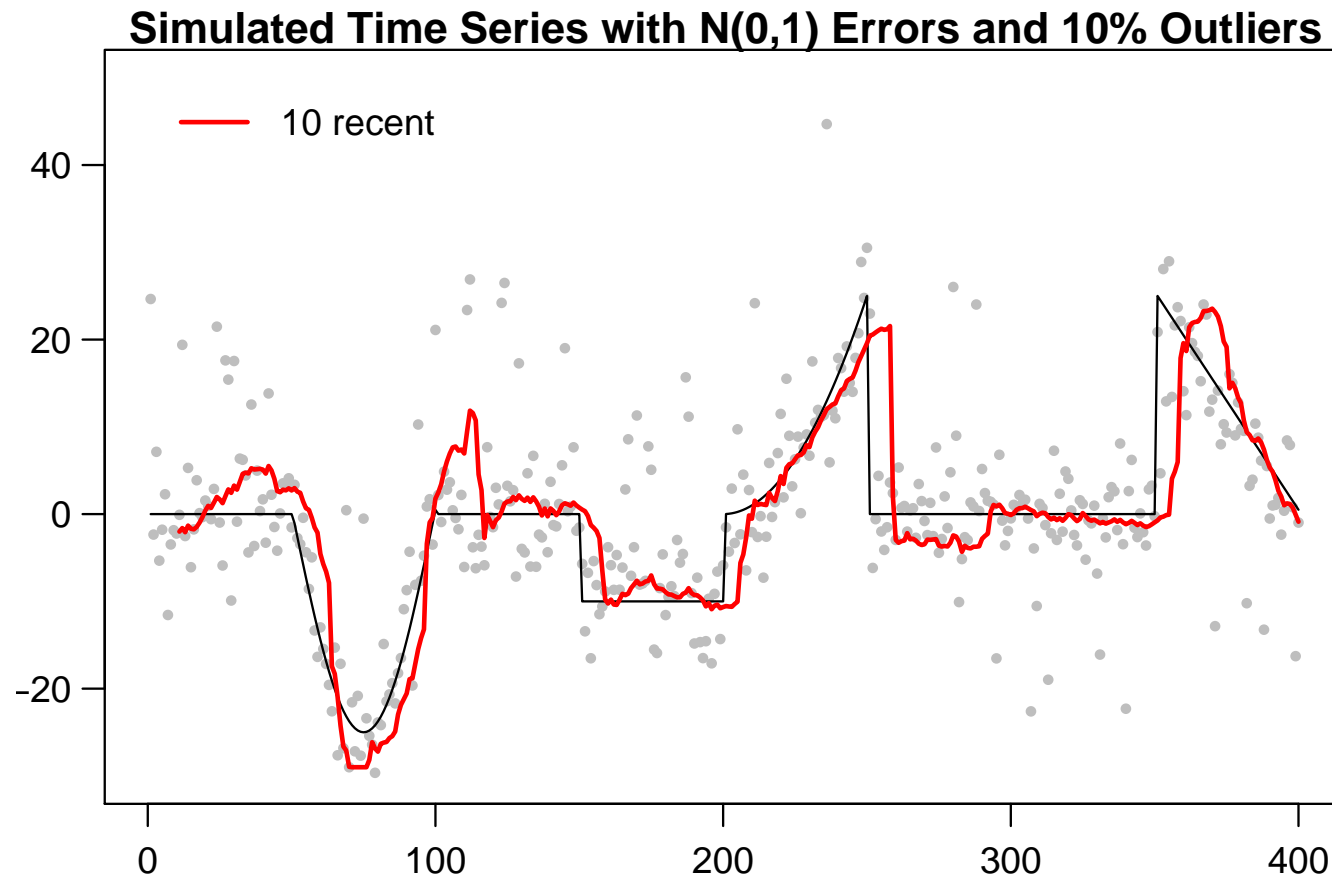
Best performance: I containing most recent time points

Application - Simulated Time Series

Simulated Time Series with $N(0,1)$ Errors and 10% Outliers



Application - Simulated Time Series



Best performance: I containing most recent time points
 n_I small and independent of n

II. Multivariate Signal Extraction

Model: Signal Extraction for Multivariate Time Series

(Lanius, Gather, 2007)

Signal + noise model

$$\mathbf{x}(t) = \boldsymbol{\mu}(t) + \boldsymbol{\varepsilon}(t) + \boldsymbol{\nu}(t) , \quad t \in \mathbb{N}$$

$\boldsymbol{\mu}(t) = (\mu_1(t), \dots, \mu_k(t))^T$ k -variate signal

$\boldsymbol{\varepsilon}(t) \in \mathbb{R}^k$ errors

$\boldsymbol{\nu}(t) \in \mathbb{R}^k$ outlier generating process

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$\boldsymbol{\varepsilon}(t) \in \mathbb{R}^k$ errors

$\boldsymbol{\nu}(t) \in \mathbb{R}^k$ outlier generating process

Assumption: Each component $\mu_j(t)$, $j = 1, \dots, k$, is locally linear

Idea

Approximate signal vector $\boldsymbol{\mu}(t)$

within each time window $\{\mathbf{x}(t-m), \dots, \mathbf{x}(t), \dots, \mathbf{x}(t+m)\}$

by k lines

Model: Signal Extraction for Multivariate Time Series

Local linear model within a time window of length $n = 2m + 1$:

$$\mathbf{x}(t + i) = \boldsymbol{\mu}(t) + \boldsymbol{\beta}(t) i + \boldsymbol{\varepsilon}(t, i) + \boldsymbol{\eta}(t, i), \quad i = -m, \dots, m$$

- Estimation of the current level by $\hat{\boldsymbol{\mu}}(t)$ in centre
- Use multivariate regression method which is
 - fast to compute
 - affine equivariant (ideally)
 - highly robust

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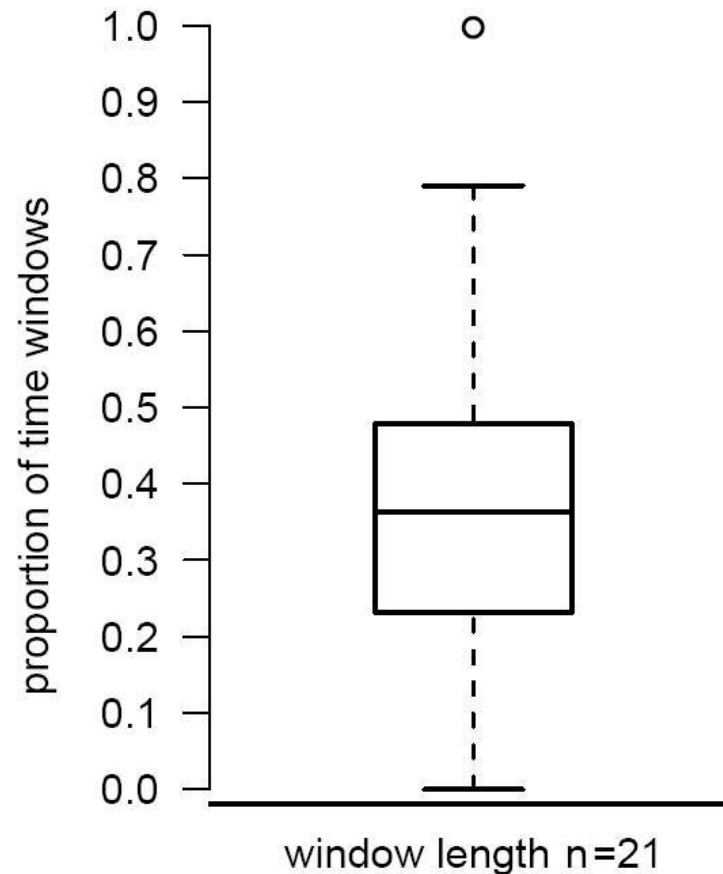
- Estimation of the current level by $\hat{\boldsymbol{\mu}}(t)$ in centre
- Use multivariate regression method which is
 - fast to compute
 - affine equivariant (ideally)
 - highly robust (breakdown point of approx. 50%).

This affords the data to be in general position.

Data Situation

Haemodynamic variables
measured on discrete scale

⇒ Observations
not in general position:



On average the estimated MCD covariance matrix
implodes in 30-40% of all time windows

Comparisons: Multivariate Regression Techniques

Local linear model for each t , $t = m + 1, \dots, T - m$:

$$\mathbf{x}(t + i) = \boldsymbol{\mu}(t) + \boldsymbol{\beta}(t) i + \boldsymbol{\varepsilon}(t, i) + \boldsymbol{\eta}(t, i), \quad i = -m, \dots, m$$

Regression Method	Affine Equivariance	Optimal Breakdown Point	Computation
Least Squares	+	0	✓
Generalisation of robust univariate approaches	-		✓
	-		✓
	-		✓
MLTS Regression	+		approximative
MCD Regression	+		approximative

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Regression Method	Affine Equivariance	Optimal Breakdown Point	Computation
Least Squares	+	0	✓
Generalisation of robust univariate approaches	L_1	$\sim 1/3$	✓
	LMS	$\lfloor n/2 \rfloor / n$	✓
	RM	$\lfloor n/2 \rfloor / n$	✓
MLTS Regression	+	$\lfloor (n - k)/2 \rfloor / n$	approximative
MCD Regression	+	$\lfloor (n - k)/2 \rfloor / n$	approximative

Procedure for Multivariate Signal Extraction

(Lanius, Gather, 2007)

Within each time window $\{\mathbf{x}(t + i), i = -m, \dots, m\}$:

1. Use univariate **RM** to find $\hat{\mu}_j(t)$ and $\hat{\beta}_j(t)$ for each j

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Procedure for Multivariate Signal Extraction

(Lanius, Gather, 2007)

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5. Calculate $\hat{\boldsymbol{\beta}}^{\text{new}}(t)$ and $\hat{\boldsymbol{\mu}}^{\text{new}}(t)$ by Least Squares Regression based on $\{(t+i, \mathbf{x}(t+i)), i \in I_t\}$

Properties

- Very robust procedure (optimal breakdown point of 50%)
- Procedure is not affine equivariant, but:
with correlated errors more efficient than univariate methods
and affine equivariant methods with similar breakdown point
- Fast computation
- Applicable to discrete data

Also: Online version with adaptive window width!

Adaptive Multivariate Online Signal Extraction

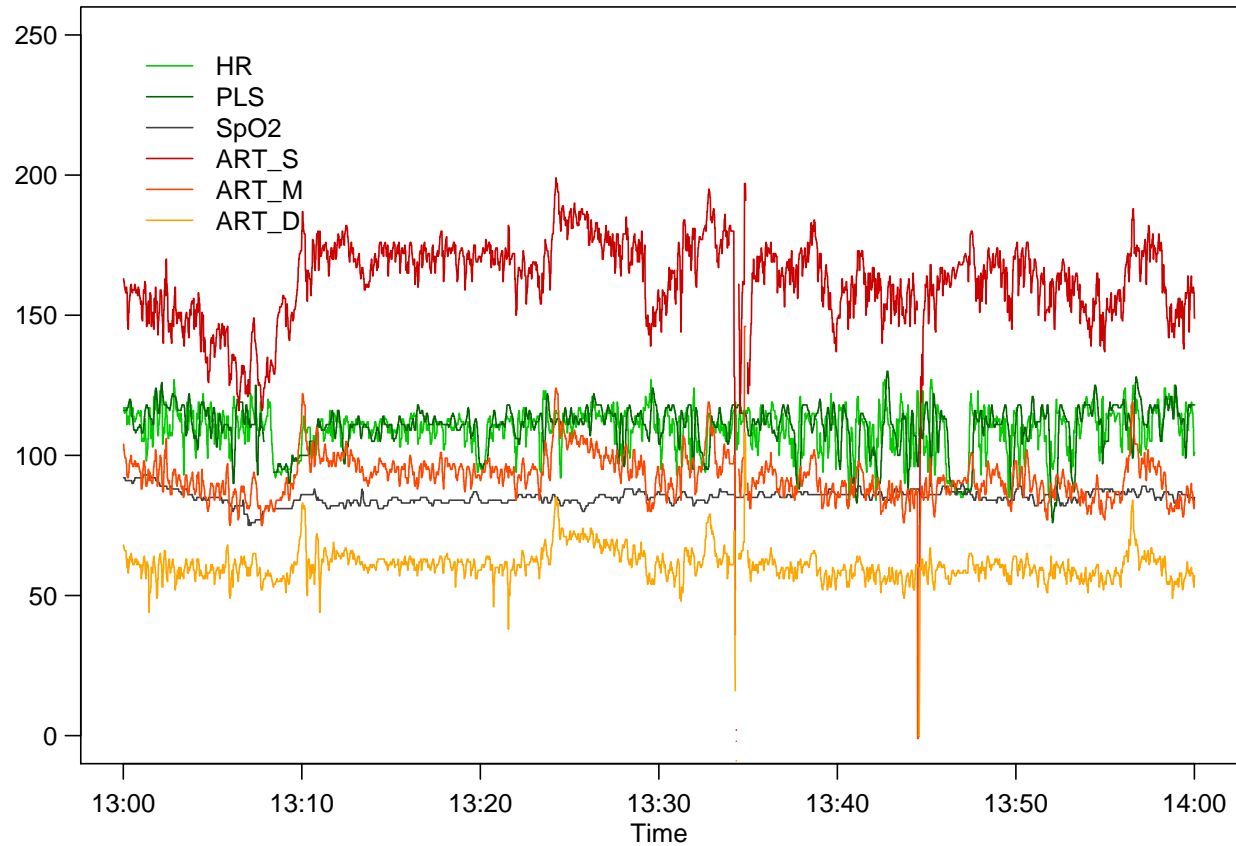
(Borowski, Schettlinger, Gather, 2008)

Within each time window $\{\mathbf{x}(t+i), i = -n(t-1), \dots, 0\}$:

1. **Use adaptive univariate RM** to find $\hat{\mu}_j(t)$ and $\hat{\beta}_j(t)$ for each j and **determine new window width $n(t)$**
2. Find residuals $\mathbf{r}(t+i) = \mathbf{x}(t+i) - \hat{\boldsymbol{\mu}}(t) - i\hat{\boldsymbol{\beta}}(t)$
3. Use modified OGK_{Q_n} -estimator as robust estimate of the local covariance matrix $\boldsymbol{\Sigma}(t)$ of $\mathbf{r}(t+i)$
4. Find $I_t = \{i = -n(t)+1, \dots, 0 : \mathbf{r}(t+i)^\top \hat{\boldsymbol{\Sigma}}(t)^{-1} \mathbf{r}(t+i) \leq d_{n(t)}\}$
5. Calculate $\hat{\boldsymbol{\beta}}^{\text{new}}(t)$ and $\hat{\boldsymbol{\mu}}^{\text{new}}(t)$ by Least Squares Regression based on $\{(t+i, \mathbf{x}(t+i)), i \in I_t\}$

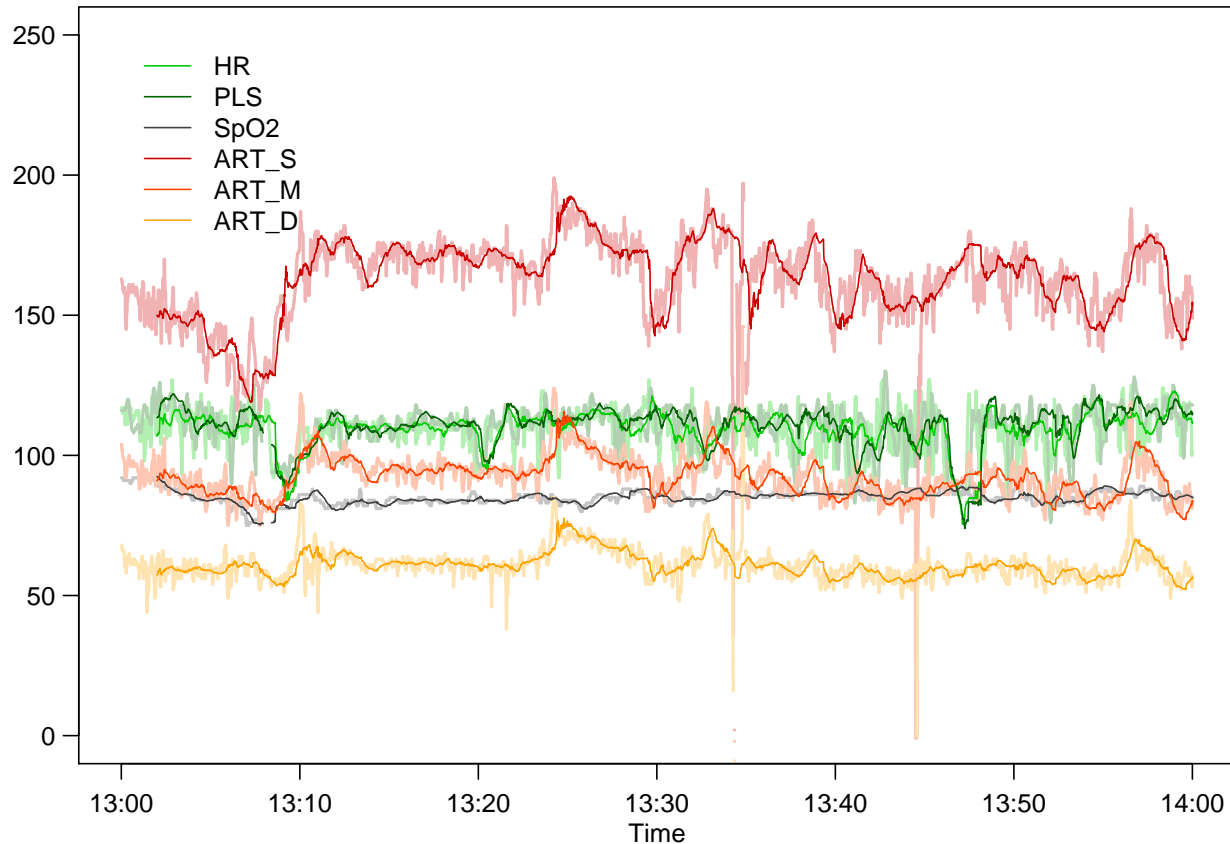
Comparison: Application to Multivariate Time Series

Multivariate Physiological Time Series



Comparison: Application to Multivariate Time Series

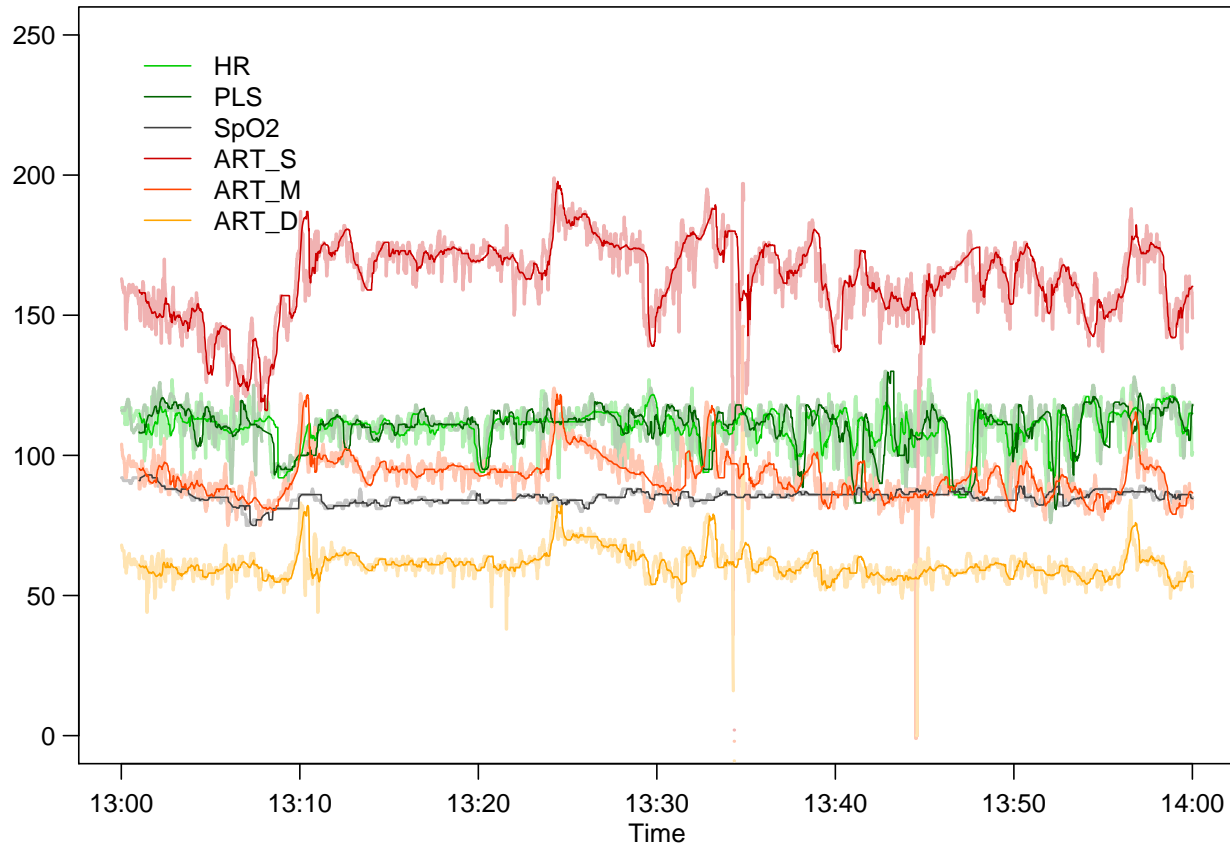
Multivariate TRM-LS Estimation



- Smooth
- Large delay at sudden changes and shifts

Comparison: Application to Multivariate Time Series

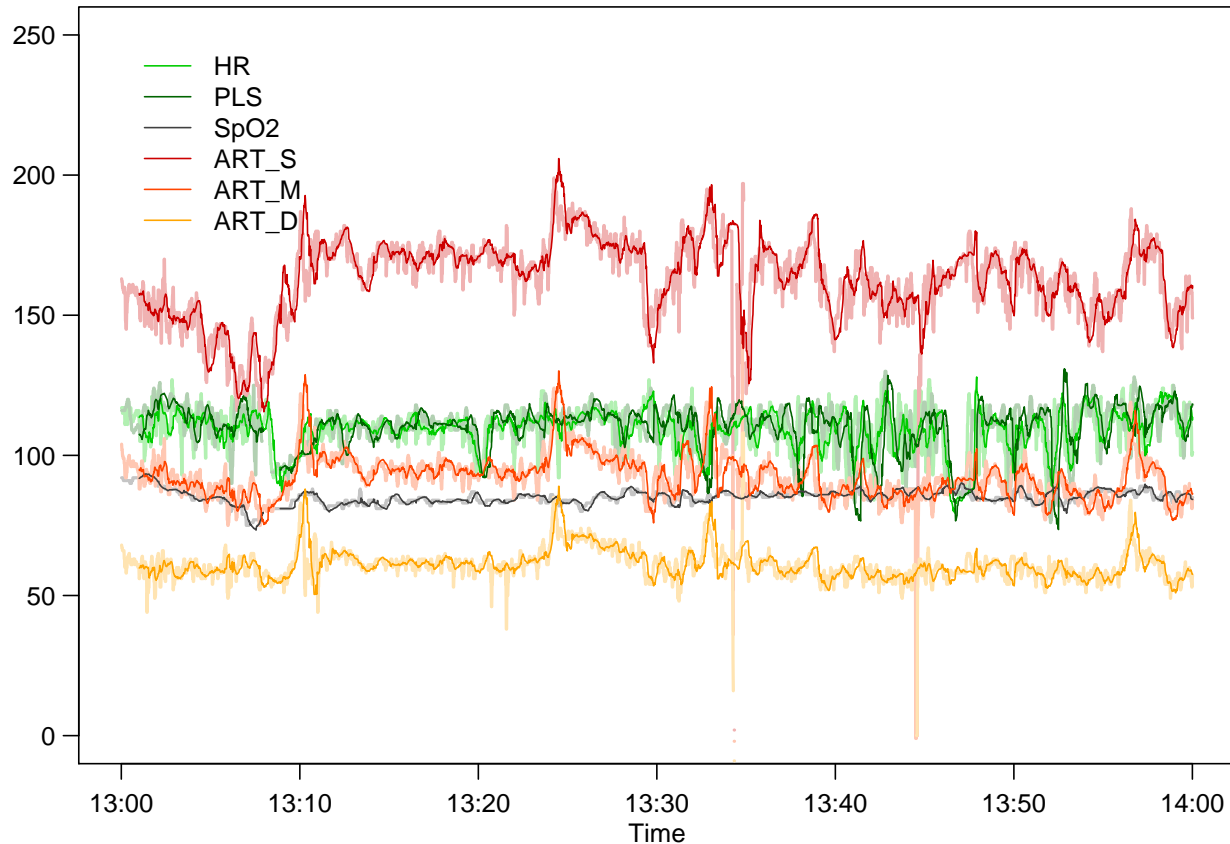
Univariate Adaptive RM Estimation



- Small delay at sudden changes and shifts
- Does not take covariance structure into account

Comparison: Application to Multivariate Time Series

Multivariate Adaptive TRM-LS Estimation



- Small delay at sudden changes and shifts
- Takes covariance structure into account

Summary

- Fast computation
- Robust (50% breakdown point)
- Adapts to sudden changes quickly
- Takes covariance structure into account
- Application to discrete data with missing values possible
- Additional rules against over- / underestimation of the signal

III. Alarm Classification

Intensive Care Data

Physiological variables

- Respiratory rate, oxygen saturation
- Arrhythmia indicator
- Heart rate, pulse
- Arterial systolic, diastolic and mean blood pressure
- Temperature

Thresholds

Alarm information from the monitor (alarm grade)

The Most Frequent Alarms

variable	alarm frequency	without manipulation	
		non alarm relevant	alarm relevant
ART S	1678	602	232
SpO2	1595	491	363
HR	453	311	59
ARR	263	210	15
ART M	268	123	43
RESP	218	168	2

In total: 4747 alarms in 780 hours recording

Consequences of Misclassification

Situation is **alarm relevant** but classified as **non alarm relevant**

- Possibly serious danger to health or life
- Control the probability of misclassifying alarm relevant situations

Consequences of Misclassification

Situation is **alarm relevant** but classified as **non alarm relevant**

- Possibly serious danger to health or life
- Control the probability of misclassifying alarm relevant situations

Situation is **non alarm relevant** but classified as **alarm relevant**

- Annoyance
- Minimise the probability of misclassifying non alarm relevant situations

Solution: Random Forest

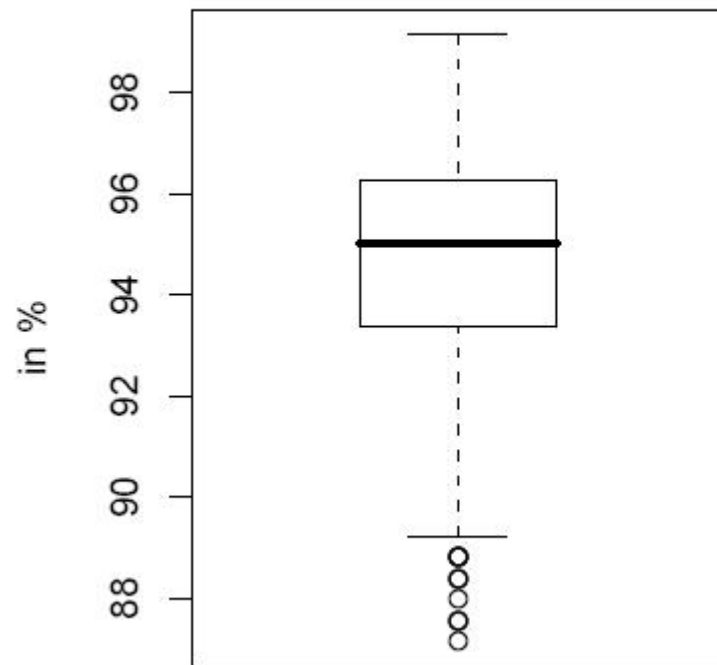
Construction of a forest (ensemble of decision trees)

- Divide the sample into three sets: learning, estimation and test set
- Build a forest of 1000 trees on the learning set
- Estimate the distribution of the test statistic on the estimation set
- Find the critical value for the test
- Apply the forest to the test set

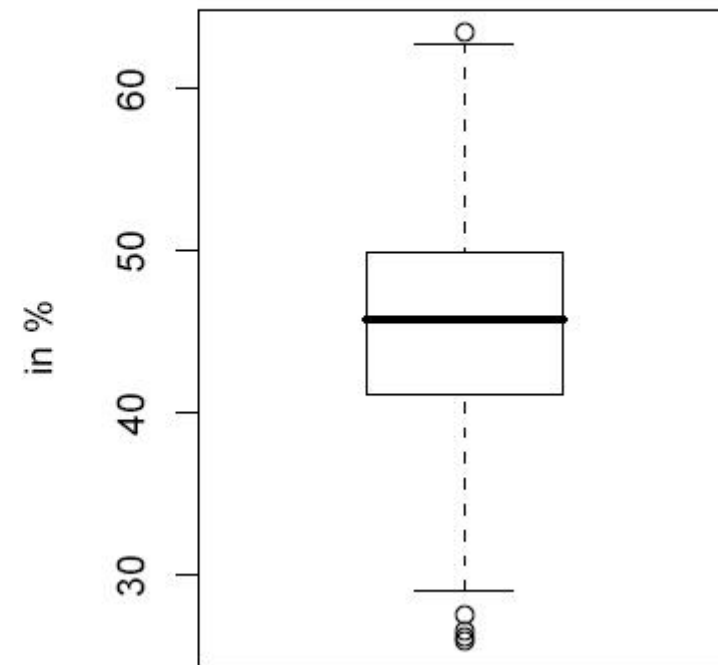
➔ Repeat this 1050 times.

Results – Significance Level 5%

Sensitivity



False alarm reduction



Mean sensitivity: **94.7%**

Mean false alarm reduction: **45.6%**

Conclusions and Future Plan

- Combine forests with Repeated Median filtering
- Combine then with alarm delay:
if decided not to alarm wait 15 seconds and think again
(Charbonnier, Badji, Gentil, 2005)
- Implement into alarm system

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Intelligent patient monitoring system

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